



Diagnosis of Cervical Cancer using Global and Local Shape Features

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ABSTRACT: The main objective of this paper is to diagnose the cervical cancer at earlier stage using pap smear images. It is performed by explicit use of shape features. Segmentation of pap smear cell image is carried out using active contour model. The segmented pap smear images are encoded with global and local shape features. The global and local shape features are combined and then feature selection is performed by applying sequential floating forward selection method. BPNN and SVM classifiers are utilized. Results show that SVM classifier yields better accuracy than BPNN classifier for diagnosis of cervical cancer.

KEYWORDS: Cervical cancer, Classification, Feature selection, Segmentation, Shape features

I. INTRODUCTION

Cervical cancer is the second common type of cancer among women all over the world. It is believed that the human papilloma virus (HPV), more specifically HPV 16 and HPV 18 type of viruses are the main constraints for the formation of cervical cancer. Screening tests are used to diagnose the cervical cells whether they are normal or abnormal. Life of the patients can be saved by early diagnosis. For early diagnosis, regular screening tests are required for women. Developing countries like India still have lack of awareness. So, the cervical cancer affected patients are more in India while comparing with developed nations. In order to conduct more screening test, an automated diagnosis method is necessary because manual diagnosis may take more time and more skilled man power. Recent years, lots of computer aided diagnosis (CAD) methods are developed rapidly to assist doctors in confirmative diagnosis. All these methods have its own merits and demerits. Still more researches are required to improve the reliability and accuracy of diagnosis. Shape features can be divided as local and global shape features. Global features represent the whole image and local features encode the specific region of an image. In this work, cervical cancer diagnosis method is presented using both shape features.

The paper is organized as follows. Section 2 briefs about related works. Section 3 presents the methodology. Section 4 deals with results and discussion. Section 5 concludes the work.

II. RELATED WORK

Dibet Garcia-Gonzalez et al (2016) presented a new method to segment nucleus in pap smear images which combines segmentation and classification algorithms. Loris Nanni et al (2015), Edwin Jayasingh Mariarputham et al (2015) and Sukumar P et al (2015) discussed SVM based classification methods for cervical cancer. Yessi Jusman et al (2014) utilized ANN, SVM, kNN and LDA classifiers. Thanatip Chankong et al (2014) and Lili Zhao et al (2016) suggested new methods for cervical cancer cell segmentation. Siti Noraini Sulaiman et al (2015) proposed clustering algorithm to segment pap smear images into the nucleus, cytoplasm and background regions. Sayeda, Ahmed M et al (2016) implemented classification of breast tumors using magnetic resonance images. Ayubu Hassan Mbagha et al (2014) applied support vector machine based on recursive feature elimination.

Nagarajan,G. et al (2016) presented about medical image feature extraction and selection. Bolon-Canedo, V., et al (2014) reviewed the most recent feature selection methods developed in this field and presented medical binary dataset

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contains various cancers. Jothi G et al (2016) performed supervised feature selection for MRI brain tumor image classification. Meenakshi M. Kavitha R et al (2014) implemented segmentation and classification for cervical cells. Rabindra Kumar Singh et al (2015) reviewed the feature selection techniques based cancer classification and also the predominant role of SVM for cancer classification. Barnali Sahoo et al (2012) performed feature selection using particle swarm optimization for cancer microarray data. Anousouya Devi, M. et al (2016) and Xiaoping Qiu et al (2007) implemented classification of normal or abnormal cells of cervical cancer using ANN. Konstantina Kourou et al (2015) conducted a reviewed machine learning algorithms such as ANN and SVM for cancer prognosis.

III. METHODOLOGY

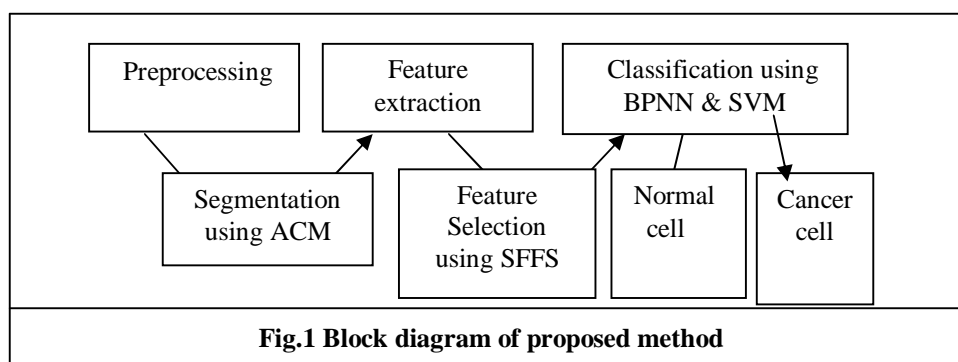


Fig.1 depicts the block diagram of the proposed method.

A. DATASET

To implement the method of this research work, the dataset is obtained from Rajah Muthiah Medical College & Hospital, Annamalai University, Annamalainagar. The dataset contains 480 cervical cell images.

B. SEGMENTATION

Image preprocessing is the first procedure in image processing which involves gray scale conversion, noise or artifacts removal and image enhancement. Segmentation is a method which subdivides an image into regions. Segmentation accuracy decides the eventual success or failure of computerized analysis procedures. In this work, active contour model is applied for segmentation. Active contour model is a process to obtain a segmented object. Active contour is a energy-minimizing spline guided by external constraint forces. Active contour is also known as snakes which is a framework for getting object. The framework minimizes an energy associated to the current contour as a sum of internal and external energies. External energy expression is derived such that it is low at object boundary. Internal energy regulates the shape of contour controlling its curvature and shape regularity. Autonomous and self-adapting in their search for minimal energy is the main advantage of snakes. The contour is defined in the (x, y) plane of an image and position of the snake $V(S) = (x(s) + y(s))$ energy function is given as

$$E_{snake}^* = \int_0^1 E_{snake}(V(S)) ds \quad (1)$$

$$= \int_0^1 E_{int}(V(S)) + E_{image}(V(S)) + E_{con}(V(S)) ds \quad (2)$$

where E_{int} is internal energy of the spline due to bending, E_{image} is rise to the image forces and E_{con} is rise to the external constraint forces.

It is shown in the Fig.2, images $(a_1 - c_1)$ show the original image. Images $(a_2 - c_2)$ are the gray scale image of $(a_1 - c_1)$ respectively. Image (a_3) depicts the user made curve which is very near to nucleus boundary. The image (a_4) displays the segmented image of nucleus. In the same manner, the images $(b_3 - b_4)$ and $(c_3 - c_4)$ are shown the various stages in nucleus segmentation. In Fig.3, the images d_1 and e_1 are the original images. d_2 and e_2 are the respective gray scale images. d_3 and e_3 show the curvature very close to the cytoplasm boundary. d_4 and e_4 in Fig.3 are the segmentation of cytoplasm. The contours slide while minimizing their energy, high level computation can activate with the contour model by forcing it toward an appropriate local minimum. The curvature then starts deforming and moving towards the desired object boundary. At the end, it completely shrink-wraps around the object. The segmentation quality highly depends on the image. Clear gray level objects are suitable for the best quality of segmentation.

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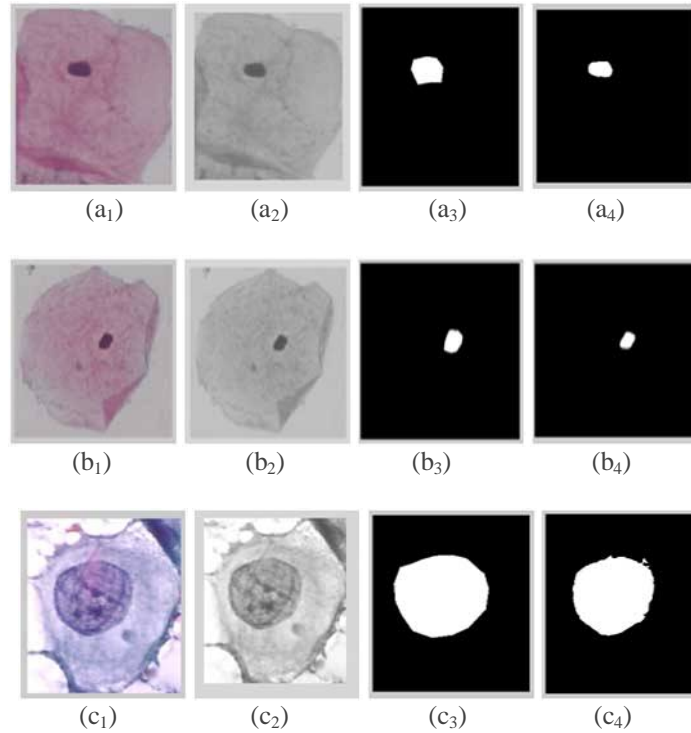


Fig. 2 Nucleus Segmentation using Active Contour Model

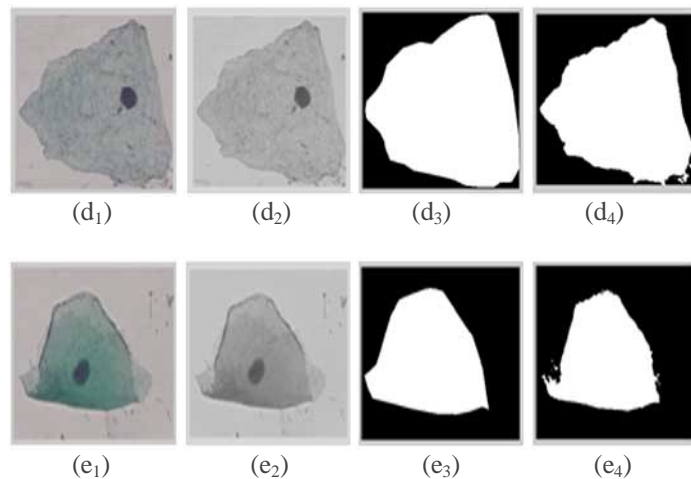


Fig. 3 Cytoplasm segmentation using Active Contour model

C. LOCAL SHAPE FEATURES

Local shape feature is the representation or encoding of a specific region of an image. Several local shape features are required to encode an image. In this work, nucleus and cytoplasm based local shape features are extracted. The ratio of nucleus and cytoplasm is given as

$$\text{Nucleus-Cytoplasm ratio} = \frac{\text{Nucleus}_{\text{area}}}{\text{Nucleus}_{\text{area}} + \text{Cytoplasm}_{\text{area}}} \quad (3)$$

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Nucleus longest diameter and Cytoplasm longest diameter is calculated as the longest distance between two pixels on the objects border. Nucleus shortest diameter and cytoplasm shortest diameter is defined as the biggest diameter a circle can have when the circle is totally inscribed in the object. Elongation of nucleus is given by

$$Nucleus_{elong} = \frac{Nucleus_{short}}{Nucleus_{long}} \quad (4)$$

Elongation of cytoplasm is given by

$$Cytoplasm_{elong} = \frac{Cytoplasm_{short}}{Cytoplasm_{long}} \quad (5)$$

Nucleus brightness is calculated as the average perceived brightness that is a function of the colors wavelength

$$Nucleus\ Brightness = 0.299\ Red\ \mu + 0.587\ Green\ \mu + 0.114\ Blue\ \mu \quad (6)$$

Nucleus roundness is computed as

$$Nucleus_{circle} = \frac{\pi}{4} Nucleus_{long}^2 \quad (7)$$

$$Nucleus_{roundness} = \frac{Nucleus_{area}}{Nucleus_{circle}} \quad (8)$$

$$Nucleus_{position} = \frac{2a\sqrt{(x_{Nucleus} - x_{Cytoplasm})^2 + (y_{Nucleus} - y_{cytoplasm})^2}}{Cytoplasm_{long}} \quad (9)$$

Likewise, nucleus related features such as area, eccentricity, equidiameter, major axis length, minor axis length, convex area, perimeter, solidity, euler number, extent, orientation, centroid and cytoplasm related features such as area, eccentricity, equidiameter, major axis length, minor axis length, convex area, perimeter, solidity, euler number, extent, orientation, centroid and roundness are extracted. In this work, totally 32 local shape features are obtained.

D. MOMENT INVARIANT FEATURES

Hu, M.K., (1962) proposed seven properties related to connected region that are invariant to rotation, scaling, and translation. Hu obtained six absolute orthogonal invariants and one skew orthogonal invariant. They are independent of orientation, position, size and parallel projection. The moment invariants have been accepted to be the sufficient measures for analyzing image patterns concerned with the images translation, rotation and scaling under the assumption of images with continuous functions and noise-free.

$$\phi_1 = \eta_{20} + \eta_{02} \quad (10)$$

$$\phi_2 = (\eta_{20} - \eta_{02})^2 + 4\eta_{11}^2 \quad (11)$$

$$\phi_3 = (\eta_{30} - 3\eta_{12})^2 + (3\eta_{21} - \mu_{03})^2 \quad (12)$$

$$\phi_4 = (\eta_{30} + \eta_{12})^2 + (\eta_{21} + \mu_{03})^2 \quad (13)$$

$$\phi_5 = (\eta_{30} - 3\eta_{12})(\eta_{30} + \eta_{12})[(\eta_{30} + \eta_{12})^2 - 3(\eta_{21} + \eta_{03})^2] + (3\eta_{21} - \eta_{03})(\eta_{21} + \eta_{03})[3(\eta_{30} + \eta_{12})^2 - (\eta_{21} + \eta_{03})^2] \quad (14)$$

$$\phi_6 = \eta_{20} - \eta_{02}[(\eta_{30} + \eta_{12})^2 - (\eta_{21} + \eta_{03})^2] + 4\eta_{11}(\eta_{30} + \eta_{12})(\eta_{21} + \eta_{03}) \quad (15)$$

$$\phi_7 = (3\eta_{21} - \eta_{03})(\eta_{30} + \eta_{12})[(\eta_{30} + \eta_{12})^2 - 3(\eta_{21} + \eta_{03})^2] - (\eta_{30} - 3\eta_{12})(\eta_{21} + \eta_{03})[3(\eta_{30} + \eta_{12})^2 - (\eta_{21} + \eta_{03})^2] \quad (16)$$

ϕ_7 is the skew moment and this invariant distinguish the mirror images. The seven moment invariants are unchanged under image scaling, translation and rotation.

In this work, 32 local shape features and 7 moment invariant features, totally 39 shape features have been extracted.

E. FEATURE SELECTION

The sequential floating forward selection (SFFS) method is one of the most efficient feature selection techniques. This algorithm starts with a null feature subset. Then, the best feature in the feature set that satisfies some criterion function is added with the current feature subset. This is the main process of the sequential forward selection. Further, any improvement in the criterion is searched if some feature is excluded. By this way, the worst feature according to the criterion is eliminated from the feature subset. This is the process of sequential backward selection.

In this manner, the algorithm proceeds by adding or subtracting the number of features until the optimal feature subset is selected. The word floating denotes the increase or decrease in dimensionality of features in the selected feature subset. Let full feature set is denoted as $F = \{f_1, f_2, \dots, f_n\}$. An optimal feature subset that has to be arrived is given as $S = \{s_1, s_2, \dots, s_m\}$ where $m < n$. That is the number of selected features must be less than the full feature set. Initially the selected feature set is set to null and it is denoted as $S = \{\emptyset\}$.

Algorithm 1 shows the step by step procedure of sequential floating forward selection method.



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Algorithm 1 : Sequential Floating Forward Selection method

Input : 39 number of input features

Output : 18 number of selected features

Step 1: Input the set of all features, $F = \{f_1, f_2, \dots, f_n\}$.

Step 2: Initialize the empty feature subset $S = \{\emptyset\}$, and counter variable $k = 0$

Step 3: Select the best significant feature

$$f^+ = \operatorname{argmax}[J(S_k + f)]; f \notin S_k$$

$$S_k = S_k + f^+$$

$$k = k + 1$$

Step 4: Select the least significant feature

$$f^- = \operatorname{argmax}[J(S_k - f)]; f \in S_k$$

Step 5: If $J(S_k - f^-) > (S_k)$ then

$$S_{k+1} = S_k - f$$

$$k = k + 1$$

go to Step 4

else

go to Step 3

Step 6: Get a selected optimal subset of features S .

F. BACKPROPAGATION NEURAL NETWORK (BPNN) CLASSIFIER

Backpropagation is a training algorithm for multilayer supervised artificial neural network. Before to start training an artificial neural network, the network is built. It means that the number of nodes in the input layer, output layer and the hidden layer is defined.

In the backpropagation network, the input layer receives the input and the output layer produces the output. The network structure is given in Fig. 4.

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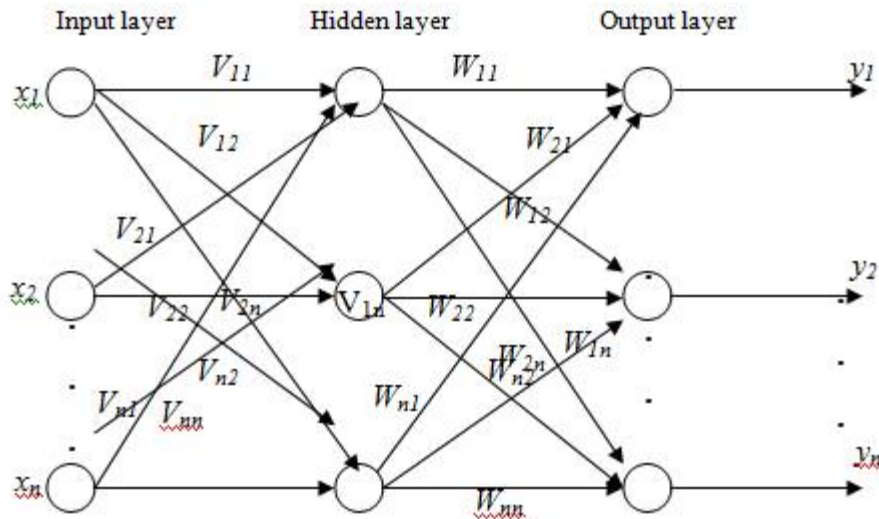


Fig. 4 Two layer backpropagation neural network.

1) Backpropagation Training Algorithm

The first step in training process is, all the weights must be assigned to small random numbers. In order to train the backpropagation network, the following steps are required:

1. The training pair from the training set is selected and the input vector is applied to the network input.
2. The output of the network is calculated using activation functions.
3. The error between the network output and the desired output is calculated.
4. The weights of the network are adjusted in a way that minimizes the error.
5. Steps 1 to 4 is repeated for each training pair in the training set until the error for the entire set is preferably low.

The s value of each neuron in the first layer is calculated as the weighted sum of its neurons inputs. The activation function f then forces s to produce the output value o for each neuron in that layer. Once the set of outputs for a layer is calculated, it serves as an input to the next layer. This process is continuously repeated until the final layer of network output is produced. This is expressed mathematically as follows:

$$s_j = \sum_{i=1}^n x_i V_{ij} \quad (17)$$

$$o_j = f(s_j) = \frac{1}{(1 + \exp(-s_j))} \quad (18)$$

where x_i is i^{th} element of the input pattern, V_{ij} is weight from i^{th} input to j^{th} neuron in the hidden layer and s_j is the activation value of the j^{th} hidden neuron. The output of the hidden layer is given as an input to the output layer.

2) Adjusting the Weights of the Output Layer

The training process for a single weight from neuron p in the hidden layer j to neuron q in the output layer k is as follows: The output of a neuron in the output layer k is subtracted from the target value u to produce an error signal (δ). This is multiplied by the derivative of the squashing function $[o(1-o)]$ thereby producing the δ value as

$$\delta = o(1-o)(u-o) \quad (19)$$

The error value δ is multiplied by the output value from the neuron p . This product is in turn multiplied by learning rate coefficient η and the result is added to the weight. The same process is repeated for each weight proceeding from neuron in the hidden layer to a neuron in the output layer.

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$$\Delta W_{pq,k} = \eta \delta_{q,k} o_{p,j} \quad (20)$$

$$W_{pq,k}(n+1) = W_{pq,k}(n) + \Delta W_{pq,k} \quad (21)$$

where η is the training rate co-efficient, $W_{pq,k}(n)$ is the value of a weight from neuron p in the hidden layer to neuron q in the output layer at step n and the subscript k indicates that the weight is associated with its destination layer, $W_{pq,k}(n+1)$ is the value of the weight at step $n+1$ (after adjustment), $\delta_{q,k}$ is the value of the δ for neuron q in the output layer k and $o_{p,j}$ is the value of the output for neuron p in the hidden layer j .

3) Adjusting the Weights of the Hidden Layers

The Hidden layers have no target vector, so the training process described above cannot be used. Backpropagation trains the hidden layers by propagating the output error back through the network layer by layer, adjusting weights at each layer. Equations (20) and (21) are used for both output and hidden layers. During training, weights in the hidden layer operate in the reverse, passing the value of δ from the output layer to the hidden layer. Each of these weights are multiplied by the δ value of the neuron to which it connects in the output layer. The value of δ needed for the hidden layer neuron is produced by summing all such products and multiplying by the derivative of the squashing function

$$\delta_{p,j} = o_{p,j}(1-o_{p,j}) \sum_{q=1}^n \delta_{q,k} W_{pq,k} \quad (22)$$

Knowing the weights (W_{ij} 's) after training, the input patterns are fed so that ANN have the capability to recognize.

6) SVM classifier

SVM is developed in COLT-92 by Boser, Guyon & Vapnik at Bell laboratories from statistical learning theory since in 1960s. Support vectors are simply the co-ordinates in a multidimensional space. The very important training points are support vectors. They decide the hyperplane.

In Fig. 5, the SVM classification process is illustrated. The rounded objects are support vectors.

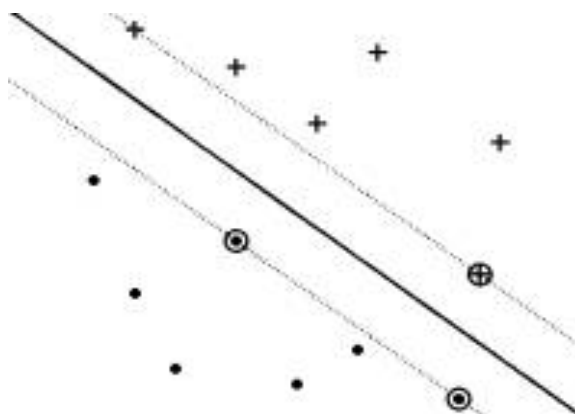


Fig. 5 SVM classifier

Fig. 5 shows the linear classification of SVM. Classifier separates the support vectors with their corresponding groups by a hyperplane. Kernels are similarity functions for machine learning algorithms. Support vector machines belong to member of kernel function. There are general purpose kernel functions and problem oriented kernel functions. In linear separable problems, the kernel functions map the training data with the high dimensional feature space. Decision function is a hyperplane in the feature space. The hyperplane for linearly separable pattern is given as

$$w^T x + b = 0 \quad (23)$$

where training set $T = \{(x_i, y_i)\}$, x_i is the input variables and y_i is the classification label. w is the weight vector and b is the perpendicular distance from the origin to the hyperplane. Separation of positive training data from negative is given as in the mathematical form

$$w^T x + b \geq 1 \text{ for } y_i = +1 \quad (24)$$

$$w^T x + b < -1 \text{ for } y_i = -1 \quad (25)$$

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Maximization of the Margin M is given as

$$M = \frac{2}{|w|} \tag{26}$$

Minimization of the margin is given as

$$M = \frac{1}{2} w^T w \tag{27}$$

In this work, BPNN and SVM is used to classify normal or abnormal cervical cancer from pap smear images.

IV. RESULTS & DISCUSSION

Feature selection using SFFS method is performed for local shape features. Out of 32 features 18 features are chosen. The number of features in the global shape features is only 7. So, feature selection is not performed for these features. Further, the local and global shape features are combined as single feature vector. By applying feature selection using SFFS method, out of 39 features 29 features are selected. Classification is performed by BPNN and SVM classifiers using the local shape features, global shape features and combined shape features with reduced features separately. The performance measure of the classifiers are analyzed in terms of accuracy, sensitivity and specificity. The accuracy is given as

1) Accuracy: Accuracy is obtained by correctly classified images divided by the classified images.

$$\text{Accuracy} = \frac{TP + TN}{(TN + TP + FP + FN)} \tag{28}$$

where TP is positive cases that are correctly identified in the dataset, TN is negative cases that are correctly classified as negative in the dataset, FP is negative cases that are incorrectly classified as positive in the dataset and FN is positive cases that are wrongly classified as negative in the dataset.

Table 1 depicts the accuracy of BPNN and SVM classifiers for local, global and combined shape features.

Table 1 Accuracy of BPNN and SVM classifiers

Sl.no	Type of features	BPNN(%)	SVM(%)
1	Local shape features	86.79	89.25
2	Global shape features	84.44	87.42
3	Combined shape features	88.49	91.16

Fig. 6 shows the accuracy level of local, global and combined features.

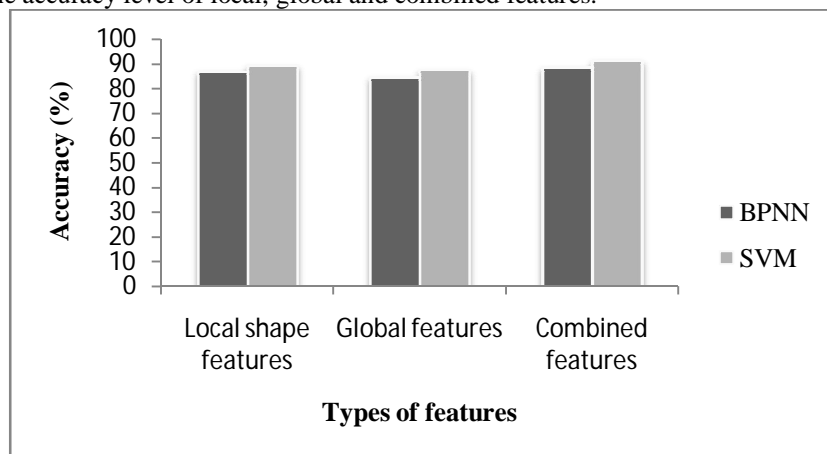


Fig. 6 Accuracy of features

2) Sensitivity: Sensitivity is obtained as correctly classified true positive rate divided by true positive and false negative samples.

$$\text{Sensitivity} = \frac{TP}{TP+FN} \tag{29}$$

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Table 2 Sensitivity of BPNN and SVM classifiers

Sl.no	Type of features	BPNN(%)	SVM(%)
1	Local shape features	85.29	87.24
2	Global features	84.78	86.53
3	Combined features	88.46	90.88

Table 2 show the sensitivity of BPNN and SVM classifiers. The higher value of sensitivity is obtained as 90.88% from SVM classifier using combined shape features.

3) Specificity: Specificity is calculated as correctly classified true negative rate divided by the true negative and false positive samples.

$$\text{Specificity} = \frac{TN}{TN+FP} \quad (30)$$

Table 3 Specificity of BPNN and SVM classifiers

Sl.no	Type of features	BPNN(%)	SVM(%)
1	Local shape features	86.49	89.29
2	Global features	84.91	86.74
3	Combined features	88.64	90.24

Table 3 displays the specificity of BPNN and SVM classifiers. The SVM classifier yields better specificity as 90.24% using combined shape features than using the features explicitly.

V.CONCLUSION

In this work, diagnosis of cervical cancer using shape features have been implemented. Local and global shape features are combined to yield better results. Feature selection is performed using SFFS method. The SVM and BPNN classifiers are applied. Performance measures such as accuracy, sensitivity and specificity are calculated. The results reveal that the SVM yields better performance than BPNN classifier as accuracy is 91.16%, sensitivity is 90.88% and specificity is 90.24%.

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BIOGRAPHY



B. Ashok was born in 1969 in India. He received his M.Sc., (Computer Science) from Bharathidasan University, Tiruchirapalli and M.Phil (Computer Science) from Annamalai University. Presently he is working as a Assistant Professor/programmer in Annamalai University. His area of research is Image processing and Data Mining. He has twenty years of experience in Application Programming. He is involved in research activities for the past seven years.



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